

Polyketal Copolymers: A New Acid-Sensitive Delivery Vehicle for Treating Acute Inflammatory Diseases

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Acute inflammatory diseases are a major cause of death in the world, and effective treatments are greatly needed. Macrophages play a central role in causing acute inflammatory diseases, and there is currently great interest in developing drug delivery vehicles that can target therapeutics to macrophages. Microparticles formulated from aliphatic polyketals have great potential to enhance the treatment of acute inflammatory diseases, due to their ability to passively target therapeutics to macrophages, their acid sensitivity, and their biocompatible degradation products. However, existing aliphatic polyketals are unsuitable for treating acute inflammatory diseases because they require weeks to hydrolyze, and strategies for accelerating their hydrolysis kinetics are greatly needed. In this report, we demonstrate that the hydrolysis kinetics of aliphatic polyketals can be accelerated by increasing their hydrophilic/hydrophobic balance. Aliphatic polyketals of varying hydrophobicity were synthesized, via the acetal exchange reaction, and their hydrolysis kinetics were investigated at the pH values of 4.5 and 7.4. A polyketal termed PK3 was developed, which had the hydrolysis kinetics suitable for treating acute inflammatory diseases. PK3 has a hydrolysis half-life of 2 days at pH 4.5, but requires several weeks to hydrolyze at pH 7.4. Microparticles were formulated with PK3, which encapsulated the anti-inflammatory drug, imatinib. *In vivo* experiments demonstrated that PK3 microparticles were able to significantly improve the efficacy of imatinib in treating acute liver failure. We anticipate that aliphatic polyketals will have numerous applications for the treatment of acute inflammatory diseases, given their pH sensitivity, tunable hydrolysis kinetics, and biocompatible degradation products.

INTRODUCTION

Acute inflammatory diseases such as acute lung injury and acute liver failure cause millions of deaths each year, and effective treatments are greatly needed (1, 2). Pro-inflammatory cytokines secreted by macrophages play a central role in mediating acute inflammatory diseases, and drug delivery vehicles that can target therapeutics to macrophages have great clinical potential (3). A key drug delivery requirement for the treatment of many acute inflammatory diseases is fast release of drugs to diseased organs, within several hours. This is because, at the time of patient diagnosis, significant tissue damage has already occurred, and organ function is rapidly deteriorating (4). It has been challenging to develop clinically acceptable drug delivery vehicles that can target therapeutics to macrophages and release them rapidly. Liposomes are a potential delivery vehicle for treating acute inflammatory diseases, due to their ability to target macrophages (5). However, their serum instability and poor storage properties have slowed their progress in clinical trials. Microparticles, based on biodegradable polymers, also have potential to enhance the treatment of acute inflammatory diseases. Microparticles can be freeze-dried, have an excellent shelf life, and can also passively target therapeutics to macrophages (6, 7). However, currently used biomaterials for drug delivery are predominantly

based on polyesters, which are potentially problematic for treating acute inflammatory diseases because of their slow hydrolysis kinetics and acidic degradation products, which themselves frequently cause inflammation (8, 9).

Microparticles formulated from polyketals are a new drug delivery vehicle, which degrade into neutral compounds comprising acetone and diols, and should therefore avoid the inflammatory problems associated with polyester-based materials (9–13). At present, only two polyketals have been synthesized for drug delivery, poly(1,4-phenyleneacetone dimethylene ketal) (PPADK) and poly(cyclohexane-1,4-diyl acetone dimethylene ketal) (PCADK) (12, 13). PPADK has excellent hydrolysis kinetics for treating acute inflammatory diseases, having a half-life of 35 h at pH 5.0, but degrades into benzene dimethanol, a compound with potential toxicity, due to its aromatic ring. PCADK is an aliphatic polyketal, which degrades into acetone and 1,4-cyclohexanedimethanol, both of which have excellent biocompatibility. However, PCADK has a hydrolysis half-life of 24 days at pH 4.5, which is too slow for applications involving the treatment of acute inflammatory diseases, and therefore strategies that can accelerate its hydrolysis kinetics are greatly needed.

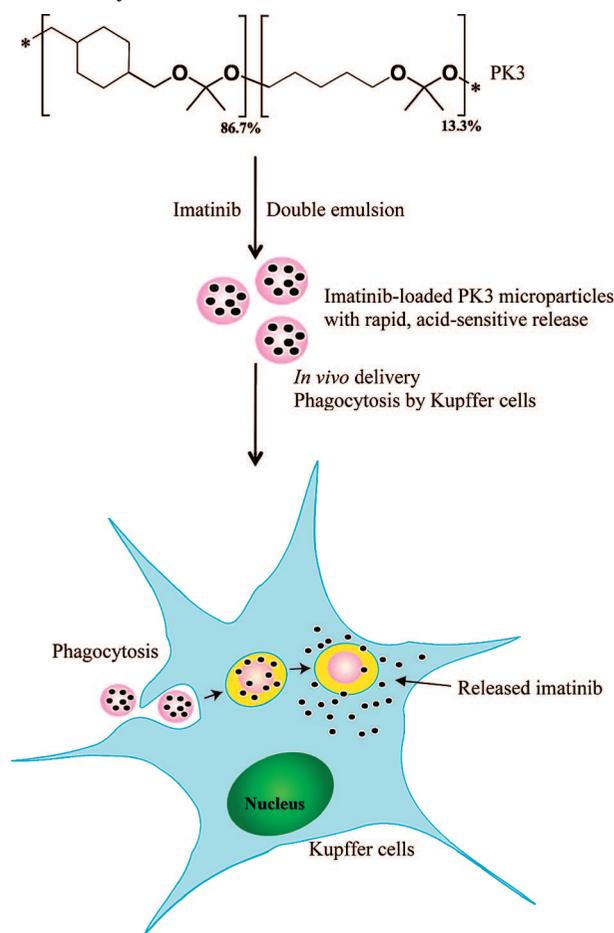
In this report, we demonstrate that the hydrolysis kinetics of PCADK derived aliphatic polyketals can be accelerated by increasing their hydrophilic/hydrophobic balance. Using this principle, we were able to generate a polyketal copolymer, termed PK3, which had a hydrolysis half-life of 2 days at pH 4.5 but several weeks at pH 7.4. Microparticles formulated from PK3 should be suitable for treating acute inflammatory diseases because they should hydrolyze and release therapeutics rapidly in the phagolysosomes of macrophages, but remain stable at

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Scheme 1. PK3, a New Biomaterial for Treating Acute Inflammatory Diseases^a


^a PK3 is a new polyketal copolymer, which hydrolyzes rapidly at the acidic pH of the macrophage phagosome. PK3 is designed to deliver therapeutics to liver macrophages and enhance the treatment of acute liver failure. PK3 microparticles were capable of enhancing the delivery of imatinib in mice suffering from acute liver failure.

physiological pH. PK3 was used to generate microparticles 1–3 μm in size, which encapsulated the NF κ B inhibitor imatinib, using a solvent evaporation procedure. The therapeutic efficacy of these PK3-imatinib microparticles was investigated in mice, using a Concanavalin A (Con A) model of acute liver failure (Scheme 1). The results from these experiments demonstrate that imatinib-loaded PK3 microparticles significantly enhanced the therapeutic efficacy of imatinib, presumably due to their accumulation in liver macrophages (Kupffer cells). Based on these results, we anticipate that aliphatic copolyketals will have numerous applications for the treatment of acute inflammatory diseases.

EXPERIMENTAL SECTION

Materials. All chemicals were purchased from Sigma-Aldrich (St. Louis, MO) and were used as received unless otherwise specified. Benzene and 2,2-dimethoxypropane were purified by distillation. Imatinib was a gift from Novartis.

Animals. Male C57/BL6 mice were purchased from Jackson Laboratory (Bar Harbor, ME). All animal experiments were approved by the Institutional Animal Care and Use Committee (IACUC) of the University of Rochester Medical Center.

Synthesis of Polyketal Copolymers. Polyketal copolymers were synthesized in a 25 mL two-necked flask, connected to a short-path distilling head. The diols, 1,4-cyclohexanedimethanol (1.04 g, 7.25 mmol) and 1,4-butanediol, 1,5-pentanediol, 1,6-

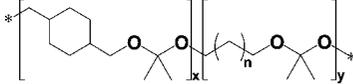
hexanediol, or 1,8-octanediol, were dissolved in 20 mL of distilled benzene and kept at 100 °C. Recrystallized *p*-toluenesulfonic acid (5.5 mg, 0.029 mmol) was dissolved in ethyl acetate (500 μL) and added to the benzene solution. The ethyl acetate was distilled off, and the polymerization reaction was initiated by the addition of 2,2-dimethoxypropane (equimolar to the two diols combined). Additional doses of 2,2-dimethoxypropane (500 μL) and benzene (2 mL) were subsequently added to the reaction, every hour for six hours, via a metering funnel, to compensate for 2,2-dimethoxypropane and benzene that had distilled off. After 24 h, the reaction was stopped with triethylamine (100 μL). The copolymers were isolated by precipitation into cold hexanes and analyzed by ¹H NMR and GPC. In general, the resulting polymers had number average molecular weights between 2000 to 3000 Da. Table 1 lists the compositions and molecular weights of the polyketal copolymers synthesized. ¹H NMR spectra were obtained from a Varian Mercury VX 400 MHz NMR spectrometer (Palo Alto, CA) using CDCl₃ as the solvent. PK1 ¹H NMR (400 MHz, CDCl₃, δ): 3.4–3.18 (m, 4H, CH₂), 1.66 (s, 1.9H, CH), 1.85–0.93 (m, 8H, CH₂), and 1.32 (s, 6H, CH₃). PK2 ¹H NMR (400 MHz, CDCl₃, δ): 3.4–3.18 (m, 4H, CH₂), 1.66 (s, 1.8H, CH), 1.85–0.93 (m, 8H, CH₂), and 1.32 (s, 6H, CH₃). PK3 ¹H NMR (400 MHz, CDCl₃, δ): 3.4–3.18 (m, 4H, CH₂), 1.64 (s, 1.7H, CH), 1.85–0.93 (m, 8.2H, CH₂), and 1.32 (s, 6H, CH₃). PK4 ¹H NMR (400 MHz, CDCl₃, δ): 3.4–3.18 (m, 4H, CH₂), 1.68 (s, 2H, CH), 1.85–0.93 (m, 8H, CH₂), and 1.32 (s, 6H, CH₃). PK5 ¹H NMR (400 MHz, CDCl₃, δ): 3.4–3.18 (m, 4H, CH₂), 1.67 (s, 1.8H, CH), 1.85–0.93 (m, 8H, CH₂), and 1.32 (s, 6H, CH₃). PK6 ¹H NMR (400 MHz, CDCl₃, δ): 3.4–3.18 (m, 4H, CH₂), 1.68 (s, 1.8H, CH), 1.85–0.93 (m, 8H, CH₂), and 1.32 (s, 6H, CH₃).

Gel Permeation Chromatography. The molecular weights of the polyketal copolymers were determined by gel permeation chromatography (GPC) using a Shimadzu system (Kyoto, Japan) equipped with a UV detector. Tetrahydrofuran was used as the mobile phase at a flow rate of 1 mL/min. Polystyrene standards (peak M_w = 1060, 2970, and 10680) from Polymer Laboratories (Amherst, MA) were used to establish a molecular weight calibration curve.

Hydrolysis of Polyketal Copolymers. The hydrolysis of the polyketal copolymers was measured according to the procedures of Lee et al. (13). Briefly, polymer samples (20 mg) were placed in buffered water (1 mL) at the pH values of 4.5 (100 mM AcOH) and 7.4 (100 mM Na₂HPO₄) at 37 °C. The polymer samples were mixed by gentle shaking and, at specific time points, were extracted into CDCl₃ (1 mL). The CDCl₃ phase was isolated and analyzed by ¹H NMR, to determine the percent hydrolysis.

Release Kinetics of Rhodamine B from PK3 Microparticles. Rhodamine B was encapsulated in PK3 microparticles using single emulsion procedures. Rhodamine B-loaded PK3 microparticles (10 mg) were suspended in pH 4.5 and pH 7.4 buffer solutions (10 mL). The suspensions were kept at 37 °C under gentle shaking. At specific time points, the suspensions (100 μL) were centrifuged at 10 000g for 2 min to remove unhydrolyzed particles. The supernatant (3 μL) was then diluted in pH 7.4 buffer (3 mL), which was then analyzed by a Shimadzu spectrofluorophotometer (Kyoto, Japan) to quantify the relative concentration of rhodamine B released from the PK3 microparticles (excitation wavelength = 556 nm, emission wavelength = 573 nm).

Formulation of Imatinib-Loaded PK3 Microparticles. Imatinib-loaded microparticles were formulated from PK3 using a modified water/oil/water emulsion method. Briefly, PK3 (100 mg) was dissolved in dichloromethane (1 mL), and in a separate vial imatinib (40 mg) was dissolved in deionized water (400

Table 1. Compositions and Molecular Weight of Polyketal Copolymers Synthesized


n = 2: PK4
n = 3: PK1, PK2, and PK3
n = 4: PK5
n = 6: PK6

polymer ID	polymer composition		M_n	PDI ^a
	monomer diol A (x)	monomer diol B (y)		
PK1	1,4-cyclohexanedimethanol (98.03%)	1,5-pentanediol (1.93%)	2149	1.742
PK2	1,4-cyclohexanedimethanol (92.46%)	1,5-pentanediol (7.56%)	2530	1.629
PK3	1,4-cyclohexanedimethanol (86.70%)	1,5-pentanediol (13.30%)	2596	1.432
PK4	1,4-cyclohexanedimethanol (96.75%)	1,4-butanediol (3.25%)	2637	1.553
PK5	1,4-cyclohexanedimethanol (85.32%)	1,6-hexanediol (14.68%)	2122	1.538
PK6	1,4-cyclohexanedimethanol (87.31%)	1,8-octanediol (12.69%)	2181	1.786

^a PDI: polydispersity index, calculated as the weight average molecular weight (M_w) divided by the number average molecular weight (M_n).

Table 2. Hydrolysis Half-Lives of Polyketal Copolymers at pH 4.5 and pH 7.4, at 37 °C

PK ID	polymer composition				half-life at pH 4.5	estimated half-life at pH 7.4	log P of diol B ^a
	diol A	percent diol A	diol B	percent diol B			
PK4	1,4-cyclohexane dimethanol	96.75%	1,4-butanediol	3.25%	1.0 day	54 days	-0.83
PK3		86.70%	1,5-pentanediol	13.30%	1.8 days	39 days	0.27
PK5		85.32%	1,6-hexanediol	14.68%	4.4 days	53 days	0.76
PK6		87.31%	1,8-octanediol	12.69%	18.6 days	360 days	1.75

^a log P is the logarithm of the water/octanol partition coefficient; the log P data were obtained from the Syracuse Research Corporation's PhysProp Database.

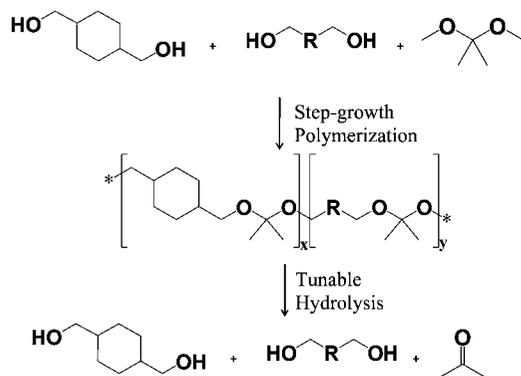


Figure 1. Synthesis of polyketal copolymers from 1,4-cyclohexanedimethanol, a second diol, and 2,2-dimethoxypropane. Hydrolysis kinetics of polyketals can be controlled by manipulating the hydrophilicity of the polyketals through copolymerizing 1,4-cyclohexanedimethanol with a more hydrophilic diol.

μL). The aqueous solution of imatinib was mixed with the PK3 solution, and sonicated for 60 s (Misonix Incorporated, Farmingdale, NY). The sonicated mixture was then immersed in liquid nitrogen for 15 s, and a 5% w/w PVA solution (pH 7.45, 12 mL) was added to it. This mixture was homogenized for 120 s with a Powergen 500 homogenizer (Fisher Scientific, Waltham, MA), and then transferred to a beaker containing 1% w/w PVA (pH 7.4, 40 mL). This solution was stirred for 3 h with a magnetic stir bar to evaporate the organic solvent. The particles were isolated by centrifuging at 10 000g for 15 min, washed twice with PBS buffer (15 mL), and freeze-dried.

Scanning Electron Microscopy (SEM). SEM images were taken to analyze the morphology of the polyketal microparticles. Briefly, SEM samples were prepared by attaching lyophilized particles onto 12.7 mm diameter aluminum sample mounting stubs (Electron Microscopy Sciences, Hatfield, PA), using conductive double-sided carbon discs (SPI Supplies, West Chester, PA). The samples were coated with a gold sputter coater (International Scientific Instruments, Prahran, Australia) for 2 min under an argon atmosphere. The SEM samples were subsequently analyzed using a Hitachi S-800 scanning electron microscope (Tokyo, Japan).

Determination of Imatinib Loading in PK3 Microparticles. The loading of imatinib in PK3 microparticles was determined by UV spectrometry. A UV calibration curve for imatinib was established at 268 nm, with a Shimadzu UV-1700 spectrometer (Kyoto, Japan) in pH 7.4 buffer. Imatinib-loaded PK3 particles were dissolved in a small amount of methylene chloride, and the imatinib was extracted into pH 7.4 buffer (100 mM Na_2HPO_4). The absorbance of both the aqueous and organic phases was measured to verify that all the imatinib was partitioned into the aqueous phase. The concentration of imatinib loaded into the PK3 microparticles was determined against the established calibration curve as mentioned above.

Treatment of Acute Liver Failure in Mice with Imatinib-Loaded PK3 Microparticles. Male C57/BL6 mice, 6–8 weeks old, were used in these studies. Appropriate doses of imatinib-PK3 particles (containing between 5 $\mu\text{g}/\text{kg}$ to 500 $\mu\text{g}/\text{kg}$ of imatinib), or an equal quantity of free imatinib, was suspended/dissolved in PBS (200 μL) and was injected intravenously using a 26 G5/8 sterilized needle. One hour later, Con A (15 mg/kg), dissolved in PBS (200 μL), was injected into the intraperitoneal cavity using a 26 G5/8 sterilized needle. Between 4 and 8 mice were used per experimental group. The mice were euthanized 8 h after the Con A injection, by cervical dislocation. Blood was then withdrawn from the heart using a 26 G5/8 sterilized needle, and kept at 4 °C overnight. The serum was isolated by centrifuging at 600g for 10 min and sent to the core facility at the University of Rochester for measurement of ALT levels.

RESULTS AND DISCUSSION

There is currently great interest in developing microparticle-based delivery vehicles that have the biocompatibility and hydrolysis kinetics needed to treat acute inflammatory diseases. Microparticles formulated from the aliphatic polyketal PCADK have excellent biocompatibility and degrade under the acidic conditions of the phagolysosome. However, the slow hydrolysis kinetics of PCADK make it unsuitable for treating acute inflammatory diseases, and therefore strategies for accelerating its hydrolysis kinetics are greatly needed. We previously hypothesized that the slow hydrolysis kinetics of PCADK was due to its hydrophobicity, making the diffusion of water into the polymer matrix the rate-limiting step in ketal hydrolysis (13). This hypothesis was based on the fact that the hydrolysis half-

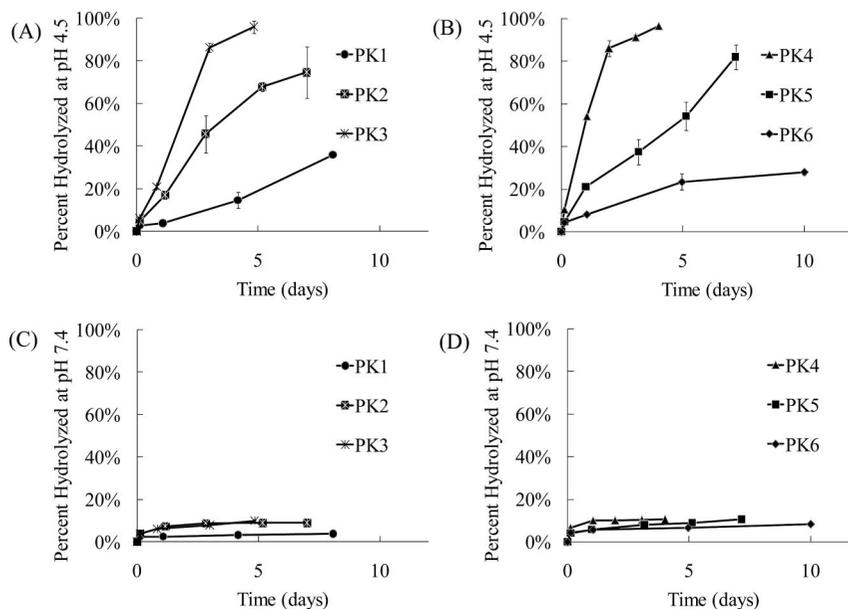


Figure 2. Hydrolysis kinetics of polyketals can be tuned by copolymerization. (A) Hydrolysis profiles of PK1, PK2, and PK3 at pH 4.5; (B) hydrolysis profiles of PK4, PK5, and PK6 at pH 4.5; (C) hydrolysis profiles of PK1, PK2, and PK3 at pH 7.4; and (D) hydrolysis profiles of PK4, PK5, and PK6 at pH 7.4. Data are presented as mean \pm standard deviation. All experiments were conducted in triplicate at 37 °C.

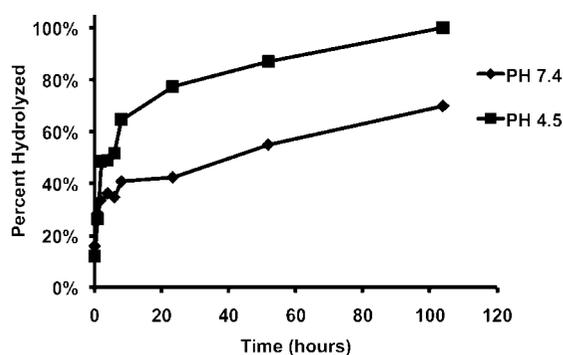


Figure 3. Release kinetics of rhodamine B encapsulated in PK3 microparticles.

life of a water-soluble dimethylacetone-based ketal is only 2 min at pH 5.0, which is 3 to 4 orders of magnitude faster than the hydrolysis of the ketal linkages in PCADK (14). Additionally, the hydrolysis kinetics of other water-insoluble polymers, such as polyanhydrides, also scale with their hydrophobicity (10). In this report, the role of hydrophobicity in governing the hydrolysis kinetics of polyketals was investigated. This was accomplished by synthesizing polyketal copolymers of varying hydrophobicity and measuring their hydrolysis kinetics.

Six polyketal copolymers were synthesized in this report (PK1–PK6, Table 1), by copolymerizing 1,4-cyclohexanedimethanol with 1,4-butanediol, 1,5-pentanediol, 1,6-hexanediol, or 1,8-octanediol. The hydrophobicity of these diols is different from that of 1,4-cyclohexanedimethanol ($\log P = 1.46$, where $P = \text{water/octanol partition coefficient}$), as evidenced by their respective $\log P$ values (Table 2). The synthesis of all the polyketal copolymers reported in this study was accomplished using the acetal exchange reaction, and was performed on a multigram scale with yields of 50–60% (Figure 1). In general, the introduction of additional diols other than 1,4-cyclohexanedimethanol did not cause any synthetic complications, and procedures developed for the synthesis of PCADK were suitable for the synthesis of all the copolymers. Importantly, all the polyketal copolymers reported in Table 1 were solid, and therefore have the potential for formulation into microparticles.

The hydrolysis kinetics of PK1 to PK6 were measured at the pH values of 4.5 and 7.4 to determine their behavior in the acidic environment of phagolysosomes and in the blood. Figure 2 demonstrates that all the polyketal copolymers (PK1–PK6) undergo acid-catalyzed hydrolysis, and that their hydrolysis kinetics scale with their hydrophilicity. PK1, PK2, and PK3 are copolymers synthesized from 1,4-cyclohexanedimethanol and 1,5-pentanediol. Their hydrophilicity scales with the amount of 1,5-pentanediol incorporated into the copolymer. This is due to the large difference in hydrophilicity between 1,5-pentanediol and 1,4-cyclohexanedimethanol, as evidenced by their respective $\log P$ values of 0.27 and 1.46. Figure 2A demonstrates that 1,5-pentanediol significantly accelerates the pH 4.5 hydrolysis kinetics of 1,4-cyclohexanedimethanol-based polyketals. For example, the hydrolysis half-life of PCADK, a homopolyketal synthesized from 1,4-cyclohexanedimethanol, is 24 days at pH 4.5 (13). On the other hand, PK3, a copolymer that incorporates 13 mol % 1,5-pentanediol and 87 mol % 1,4-cyclohexanedimethanol, had a hydrolysis half-life of only 2 days at pH 4.5. Similarly, PK2, another PCADK-derived copolymer, incorporating 7.5 mol % of 1,5-pentanediol, had a hydrolysis half-life of 3 days at pH 4.5, which is faster than PCADK but slower than PK3. PK1, the third copolymer derived from PCADK, incorporating 2 mol % 1,5-pentanediol, was only 30% hydrolyzed after 10 days at pH 4.5, which was expected based on its low incorporation of 1,5-pentanediol¹.

To determine if diols other than 1,5-pentanediol could similarly influence the hydrolysis kinetics of PCADK-derived copolymers, the hydrolysis kinetics of PK4, PK5, and PK6 were also investigated. These polyketals are PCADK-derived copolymers synthesized from 1,4-cyclohexanedimethanol and either 1,4-butanediol, 1,6-hexanediol, or 1,8-octanediol. Figure 2B,D and Table 2 demonstrate that this set of copolymers also has an inverse relationship between hydrophobicity and hydrolysis kinetics. For example, PK4, a copolymer synthesized from 1,4-cyclohexanedimethanol and 1,4-butanediol, has the

¹ Similar copolymers with higher incorporation of 1,5-pentanediol were also generated; however, those copolymers were viscous liquids, which are not suitable for formulation into microparticles for drug delivery. Therefore, we only focused our hydrolysis analysis on the solid polyketal copolymers, PK1, PK2, and PK3.

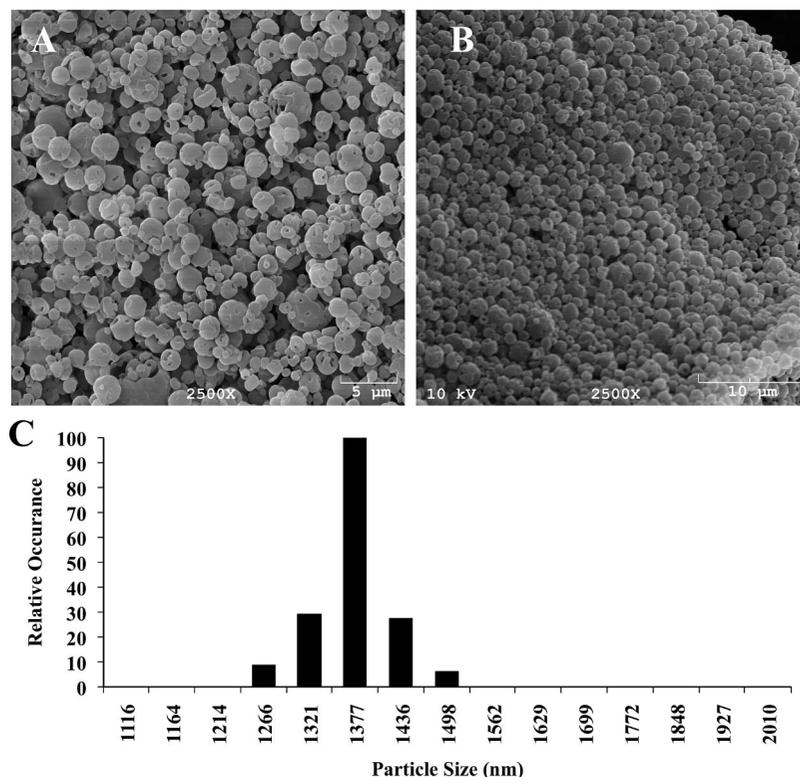


Figure 4. SEM images of particles formulated with PK3. (A) SEM image of empty particles formulated via double emulsion. (B) SEM images of imatinib-loaded PK3 microparticles formulated via double emulsion. (C) Size distribution of imatinib-loaded PK3 microparticles as determined by dynamic light scattering (DLS).

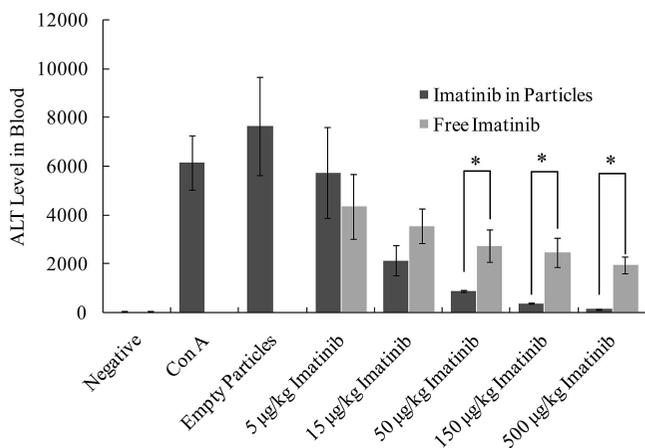


Figure 5. PK3 microparticles improve the efficacy of imatinib in treating acute liver failure in mice. Mice were injected intravenously with either imatinib or imatinib in PK3 microparticles, acute liver failure was then induced by intraperitoneal injection of Con A (15 mg/kg). Eight hours later, ALT levels in the blood were analyzed. * indicates statistical significance (Student's *t* test, $P > 0.05$, $n = 4$ to 8).

fastest hydrolysis kinetics of all the copolyketals, with a hydrolysis half-life of 1 day at pH 4.5. This is predicted based on the more hydrophilic nature of 1,4-butanediol in comparison to the other diols. On the other hand, PK6, a copolymer composed of 1,4-cyclohexanedimethanol and 1,8-octanediol, had a pH 4.5 hydrolysis half-life of 18.6 days. In summary, these data demonstrate that the hydrolysis kinetics of polyketals can be tuned by varying their hydrophilicity and further support the hypothesis that diffusion of water into the polyketals is the rate-determining step governing their hydrolysis. Importantly, the hydrolysis kinetics of all the polyketal copolymers, PK 1–6, were pH-sensitive; in general, they hydrolyzed at least 1 order of magnitude faster at pH 4.5 than at pH 7.4.

We chose PK3 for further investigation as a drug carrier for the treatment of acute inflammatory diseases because of its suitable hydrolysis kinetics and biocompatible degradation products. The copolymer PK4 has faster hydrolysis kinetics than PK3; however, it degrades into 1,4-butanediol, which is converted into γ -hydroxybutyrate *in vivo*, and subsequently causes toxicity to the central nervous system (15). Microparticles were formulated from PK3, using a solvent evaporation procedure. Figure 4A demonstrates that the size range of PK3 microparticles is between 1 and 5 μm , which is suitable for phagocytosis by macrophages.

In order to determine whether or not PK3 microparticles would have suitable drug-release kinetics for treating acute inflammatory diseases, a release study was conducted on PK3 microparticles which encapsulated the fluorescent dye, rhodamine B from PK3 microparticles is approximately 6 h at pH 4.5 and 40 h at pH 7.4, which is suitable for treating acute liver failure. The drug-release kinetics of PK3 microparticles is 20 times faster than that of PCADK microparticles, which had a release half-life of 5 days at pH 4.5 and over 15 days at pH 7.4 (data not shown).

PK3 microparticles were used to enhance the delivery of imatinib in treating acute liver failure. Imatinib is a kinase inhibitor that inhibits NF- κ B activation and has great potential for treating acute inflammatory diseases (16, 17). The activation of NF- κ B in macrophages leads to the production of cytokines and reactive oxygen species, the central causes of tissue damage during acute inflammatory diseases. Although imatinib has shown promise for treating acute inflammatory diseases in mouse models, there are also numerous side effects associated with imatinib, including heart failure and hepatic toxicity (18, 19). PK3 microparticles should enhance the efficacy of imatinib by targeting it to macrophages, thereby increasing its concentration at the target site, and also by reducing the toxic side effects of

imatinib on the heart and liver. Imatinib was encapsulated into PK3 microparticles through double emulsion procedures. These macroparticles were approximately 1.5 μm in size on average, as determined by SEM and DLS, which is suitable for delivering drugs to phagocytic cells such as Kupffer cells (Figure 4B,C). The loading of imatinib in PK3 microparticles was determined to be $0.90 \pm 0.10 \mu\text{g}$ imatinib per 1 mg of particles ($n = 3$), suggesting that the encapsulation efficiency of imatinib in PK3 microparticles was approximately 0.32%.

The ability of PK3 microparticles to enhance the delivery of imatinib was investigated in mice suffering from Con A-induced acute liver failure. Mice were injected with either imatinib in solution (0.1 μg to 10 μg of imatinib dissolved in 200 μL of saline) or an equivalent amount of imatinib loaded in PK3 microparticles (0.11 mg to 11 mg of imatinib-loaded PK3 microparticles suspended in 200 μL of saline). Acute liver failure was subsequently induced by an intraperitoneal injection of Con A. The severity of liver injury in these mice was determined by measuring the alanine aminotransaminase (ALT) level in their blood, which is a clinical surrogate marker for hepatocyte injury. Figure 5 demonstrates that PK3 microparticles enhanced the treatment efficacy of imatinib in preventing Con A-induced liver damage. For example, a dose of 500 $\mu\text{g}/\text{kg}$ of free imatinib resulted in an ALT value of approximately 2000 U, whereas 500 $\mu\text{g}/\text{kg}$ of imatinib encapsulated in PK3 microparticles reduced the ALT values to baseline levels of only 50 U. The therapeutic efficacy of 15 $\mu\text{g}/\text{kg}$ of imatinib loaded in PK3 microparticles was similar to that of 500 $\mu\text{g}/\text{kg}$ of free imatinib. These experiments demonstrate that imatinib-loaded PK3 microparticles significantly enhanced the therapeutic efficacy of imatinib, presumably due to their accumulation in liver macrophages. No noticeable toxicity was observed by injection of empty PK3 microparticles (11 mg suspended in 200 μL of saline), as shown in Figure 5.

CONCLUSIONS

In this report, we demonstrate that the hydrolysis rates of polyketals can be tuned by varying their hydrophilicity. Using this strategy, an aliphatic polyketal copolymer, PK3, was identified, which had a hydrolysis half-life of 2 days at pH 4.5, but was stable for several weeks at pH 7.4. Microparticles were formulated from PK3, which encapsulated the kinase inhibitor, imatinib, and these PK3 microparticles significantly improved the efficacy of imatinib in treating Con A-induced liver damage *in vivo*. Based on these findings, we anticipate numerous applications of copolymers of polyketals for treating acute inflammatory diseases, given their pH sensitivity, rapid and tunable hydrolysis kinetics, and biocompatible degradation products.

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